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Original Research Article

Effect of mesenchymal stem cell-incorporated hydroxyapatite-collagen scaffold on tissue repair in acute spinal cord injury, and the mechanism involved

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Abstract

Purpose: To study the effect of hydroxyapatite-collagen (HC) scaffold with mesenchymal stem cells (MSCs) on tissue repair in acute spinal cord injury (SCI).

Method: Adult female Sprague-Dawley rats weighing 200 - 230 g were randomly divided into two groups implanted either with bone marrow-MSCs (experimental group) or HC scaffold alone (control group). Spinal cord injury was induced using laminectomy, resulting in a 2.0-mm gap at T10 of the spinal cord. The gap was filled in both groups with 2-mm HC scaffold at day 10 of culture. Cellular development, viability, and proliferation inside the scaffold were determined. Angiogenesis was determined by measuring fibronectin (FN) immunofluorescence, von Willebrand factor (vWF), hypoxia-inducible factor 1-alpha (HIF-1α) and vascular endothelial growth factor (VEGF).

Results: HC scaffold strengthened MSCs. Bone marrow MSCs exhibited no statistically significant difference when compared with cells in culture at day 10 (47.03 ± 3.135 %, p > 0.05). Moreover, on days 5 and 10, FN deposition was higher in MSCs with scaffold than in scaffold-free MSCs. The expressions of FN, vWF, HIF-1 α and VEGF were positively correlated, indicating that incorporation of HC scaffold into MSCs significantly improved tissue repair by improving angiogenesis via a differentiation process (p < 0.001).

Conclusion: These findings suggest that HC scaffold with MSCs is a potential therapeutic procedure for spinal cord injury.

Keywords: Mesenchymal stem cells, Hydroxyapatite-collagen, Spinal cord injury, HC scaffold

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INTRODUCTION

Spinal cord injury (SCI) is one of the most common causes of disability worldwide. Therefore, understanding CNS pathology after SCI is key to establishing an effective treatment [1]. Currently, several lines of clinical evidence show the clinical benefits of steroids in SCI treatment. However, stem cell-based therapy has produced some exciting and beneficial effects in the management of SCI. An array of MSCs with novel and promising strategies has been established from various sources for improvement of functional recovery after SCI [2-7]. Mesenchymal stem cells (MSCs) have been shown to promote the repair of injured spinal

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cord tissues in animal models. This has generated a lot of scientific interest in the clinical use of MSCs. It is well established that MSCs have ability to secrete several types of growth factors such as cytokines, NGF, chemokines, FGF, and BDNF which improve motor functions. Preclinical studies in animal models of SCI have demonstrated that MSC transplantation improves functional recovery after SCI [4-9]. These studies also showed that MSC transplantation is safe and is beneficial to SCI patients. The MSCs are not so difficult to obtain. The major problems faced by researchers are ethical concerns with respect to the use of MSCs. Studies have demonstrated that other than replacing harmed cells, MSCs have been used in several processes such angiogenesis, as immunosuppression, neuroprotection, and foundation of a profitable microenvironment for axonal recovery [2].

Fibronectin (FN), a glycoprotein, is present in blood plasma and extracellular matrices (ECMs). The major role of FN is in cell migration and attachment via cell surface receptors [3], due to its high affinity for collagen [4]. Therefore, MSC transplantation is one of the promising methodologies for recovery of disability after line damage, through promoting spinal angiogenesis. It is not known whether the use of HC scaffold with MSCs improves tissue repair process through differentiation and angiogenesis in rats with acute SCI. Thus, the present study was designed to investigate whether the use of HC scaffold with mesenchymal stem cells would result in improved tissue repair process through differentiation and angiogenesis.

EXPERIMENTAL

Animals and human tissue

Adult female Sprague-Dawley rats weighing 200-230 g were obtained from the Laboratory Animal Center of Fujian Medical University. All experiments were performed after prior ethical approvals from the Animal Care Committee of Fujian Medical University (approval no. ACC-EC/FMU/172/12D-2018). The CPCSEA guidelines were followed for animal care in all the study-related procedures [10]. Human bone marrow MSCs (hBM-MSCs were purchased from the Department of Orthopedics, Fujian Medical University Union Hospital, Fujian, China.

Preparation of 3D hydroxyapatite-collagen scaffold for cell cultures

Commercially available hydroxyapatite-collagen graft was used as scaffold. The material is

clinically accepted as a bone graft substitute. The scaffold was sectioned into strips of 2-mm thick, round discs to facilitate nutrient delivery to the cells. The scaffold strips were decontaminated by washing with 75 % ethanol, followed by washing thrice in PBS, and soaking in culture medium for 15 min. A total of 1×10^6 cells was seeded into each HC scaffold strip and incubated at 37 °C in culture medium in a humidified atmosphere. The culture medium was replaced with fresh medium every 48 h.

Proliferation and viability of MSCs

Cellular proliferation of MSCs in scaffolds was determined using MTT assay. Scaffolds with implanted MSCs were gently taken out at each time point (days 1-10) and rinsed twice in prewarmed (37 °C) PBS solution, followed by addition of MTT solution (0.5mg/mL). The mixture was then incubated at 37 °C for 4h and the medium was discarded. Then, 300µL of DMSO was added to each well to solubilize the formazan crvstals from the scaffolds Absorbance of the solution was measured at 595 nm. A growth curve was drawn by plotting absorbance values against number of days.

Scanning electron microscopy (SEM) of scaffolds

After 10 days, cultured MSCs on HC scaffolds were washed thrice with PBS buffer solution, and then fixed in 3% glutaraldehyde for 12h at room temperature. The scaffolds were dehydrated in ethanol, air-dried, and sputter-covered with a 60nm layer of gold. They were then subjected to SEM (S-4700, Hitachi Ltd, Tokyo, Japan).

Deposition of FN on scaffolds

Western blot assay was used to determine the protein expression of FN. Onthe10th day in culture; scaffolds were rinsed severally with PBS buffer solution (PBS) and then cut into pieces using iris scissors. The pieces were further rinsed in lysis buffer containing protease and phosphatase inhibitor mixture using ultrasonic homogenizer. Polyacrylamide gel (12.5 %) was used for electrophoresis of 40 µg of protein. The protein bands were transferred to a nitrocellulose membrane. The membrane was incubated 5% BSA in a mixture of tris-buffered saline (TBS) and Polysorbate 20 (TBST) to block non-specific binding of the blot. Thereafter, the membrane was incubated with anti-FN primary antibody for 2 h. After washing with PBS, the membrane was incubated with HRP-conjugated secondary antibody for 2 h. Finally, the membrane was washed once again, and the blots were identified

with enhanced chemiluminescence (ECL). The expression of FN was normalized to that of betaactin gene which served as internal control.

Spinal cord injury model and transplantation of MSCs-scaffold

For the preparation of the SCI model, a total of 20 adult female Sprague-Dawley rats weighing 200 - 230 g were used. The rats were provided by the animal facility of Fujian Medical University, China. The animals were randomly divided into two groups, and implanted either with bone marrow MSCs (experimental groups) or HC scaffold alone (control group). Pentobarbitone anesthesia was used at a dose of 40 mg/kg, ip. Laminectomy was performed, resulting in a 2mm gap at the level of T10of the spinal cord. The gap was filled with 2-mm HC scaffolds at day 10 of culture. The gap filling was done in both the experimental and control groups. The rats received post-operation care. Once they recovered after surgery, the rats were allowed to move freely in their cages.

Immunohistochemistry

The rats were sacrificed using decapitation after the first and second months of MSCs-scaffold transplantation. The spinal cord was perfused using a solution containing 0.002 % heparin and NaNO₂, and then fixed using 4 % paraformaldehyde in phosphate buffered saline. Segments of pre-fixed spinal cord (T8-T12, 30 mm each) were incubated with the following primary antibodies: anti-HIF-1a, anti-FN, antivWF, and or anti-VEGF at 4 °C for 2h. This was followed by incubation with secondary antibody at 37 °C for 1h. The slides were observed under fluorescence microscope (Nikon, Japan). The nuclei were counterstained with Hoechst 33342 dye.

Statistical analysis

Data are presented as mean \pm SD. Statistical analysis was done using one-way ANOVA. All statistical analyses were carried out using statistical software (GraphPad Prism, version 6.0, USA). Statistical significance was assumed at *p* < 0.05.

RESULTS

Distribution of MSCs within HC scaffolds

After progressive passages, cultured MSCs turned out to be generally homogeneous. At fourth passage, the cells showed fibroblast-like structures (after achieving 80% of target. Results

from viability and proliferation using MTT assay revealed that cell population within the scaffold increased time-dependently up to 10 days (Figure 1 A). At day 10, there was no statistically significant difference in proliferation between bone marrow MSCs and cells in culture ($47.03\pm$ 3.135%, *p* > 0.05) (Figure 1 B).



Figure 1: Structural features of HC scaffolds and MSCs. Figure 1A shows cell viability of MSCs within the scaffold, as determined using MTT assay. Figure 1Bshowscomparative growth and viability of MSCs in culture disc and within the HC scaffold. Figure 1C-1E shows SEM showing multiparous structure of the HC scaffold. Figure 1E shows SEM showing adherence of MSCs to the scaffold. Scale bar (A): 40 µm. Scanning Electron Microscopy found that the cells developed into monolayers and released extracellular matrix proteins (Figure 1C-1E). On day 5 and day10, FN deposition was higher in MSCs-scaffold than in MScs without the scaffold

Western blot results

Figure 2 shows that FN deposition within the scaffold was higher on day 10 than on day 5, and FN depositions within the scaffold on day 5 and day 10 were higher than that in MSc culture flasks without scaffolds.



Figure 2: Level of FN expression, as determined using Western blot

Neovascularization

Neovascularization (angiogenesis) through expressions of HIF-1 α , vWF and VEGF was also observed. In Figure 3 A, the red fluorescence indicates the expression of vWF. The MSCs

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surrounding blood vessels expressed VEGF (green fluorescence) (Figure 3 B). Figure 3 C shows the expression of HIF-1 α .



Figure 3: Immunofluorescence showing expressions of FN, vWF, HIF-1 α and VEGF). **(A)** On day 10, FN was deposited within the GS scaffold, as revealed by red fluorescence. Red fluorescence indicates the expression of vWF; **(B)** immunostaining showing neovascularization of the graft of SCI injury site in the SCI group (green fluorescence) green fluorescence which indicates the expression of VEGF; **(C)** Expression of HIF-1 α . Scale bar: 40 µm

DISCUSSION

This is the first study designed to determine whether the use of HC scaffold with MSCs improves tissue repair process through differentiation and angiogenesis in a rat model of acute SCI. Earlier pre-clinical reports showed that MSC transplantation improved functional recovery in animal model of SCI. The present study was designed to investigate the synergistic effect of HC scaffold with MSCs in tissue repair for spinal cord injury. In this study, it was found that the use of HC scaffold was safe for patients. Indeed, this scaffold is already in use in medical practice. One more scientific advantage of HC scaffold is its affinity for cells, and its histocompatibility. Furthermore, MSCs can be sustained for 50 days in a 3D scaffold of collagen [5].

The results obtained in this study demonstrate that HC scaffold offers satisfactory availability of oxygen and nourishment *in vitro* and *in vivo* during vascularization. The possibility of developing a homogeneous situation for implantation is another basic idea for using this biomaterial. The expressions of FN, vWF, HIF-1a and VEGF were positively correlated, indicating that the addition of HC scaffold to MSCs significantly improved tissue repair by improving angiogenesis through differentiation process. These results are consistent with previous reports [6,7]. Mesenchymal stem cells (MSCs are believed to revamp their substrate by releasing extended proportions of FN and collagen (type I) to the substrate [7]. Thus, it may be assumed that the MSC-bound scaffold released FN, which was deposited on scaffold, thereby initiating angiogenesis. This is consistent with previous reports [8,9]. Biomaterial vascularization is vital because adequate perfusion of blood permits cells situated at the focal point of the scaffold to obtain enough oxygen. Studies have revealed that the expression of HIF-1 α by MSCs triggers angiogenesis [11,12]. Furthermore, it was hypothesized that decreased oxygen supply in the injured site causes lipid peroxidation and free radical generation [13].

Decreased levels of calcium, magnesium sodium and potassium enhance the expression ofHIF-1 α , and hence angiogenesis [14-16]. In summary, a 3D HC scaffold was developed in this study, and it supported the viability and proliferation of MSCs.

Moreover, it was observed that FN was deposited on the scaffold. At the point when it was transplanted to transected site of the rodent spinal cord, the scaffold was observed to be biocompatible and ready to attach to the spinal cord. Transplantation of the scaffold with MSCs advanced angiogenesis by initiating blood vessel development and expressions of HIF-1 α , vWF and VEGF in the damaged zone of the spinal cord. The 3D HC scaffold may serve as a potential supporting biomaterial for recovering motor function after SCI.

CONCLUSION

The findings of this study demonstrate that HC scaffold strengthens MSCs. This indicates that in rats with acute SCI, on addition of HC scaffold to MSCs significantly improves tissue repair process through differentiation and angiogenesis. Thus, MSC-incorporated HC scaffold is a potential remedial procedure for SCI.

DECLARATIONS

Conflict of interest

No conflict of interest is associated with this work.

Contribution of authors

We declare that this work was done by the authors named in this article and all liabilities

pertaining to claims relating to the content of this article will be borne by the authors. This paper was drafted by Zhipeng Yao. All the experiments are performed by Zhipeng Yao under supervision of Wenge Liu. Chenyang Song collected materials for this study.

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